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**D E C I S I O N**  
**of 25 January 2006**

**Case Number:** T 0504/03 - 3.2.02

**Application Number:** 96931194.3

**Publication Number:** 0796059

**IPC:** A61B 6/00

**Language of the proceedings:** EN

**Title of invention:**

Determining a dimension from a density distribution

**Applicant:**

Koninklijke Philips Electronics N.V.

**Opponent:**

-

**Headword:**

-

**Relevant legal provisions:**

EPC Art. 52(1), (4), 56

**Keyword:**

"Diagnostic method (no) "

"Inventive step (yes) "

**Decisions cited:**

-

**Catchword:**

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Case Number: T 0504/03 - 3.2.02

**D E C I S I O N**  
of the Technical Board of Appeal 3.2.02  
of 25 January 2006

**Appellant:** Koninklijke Philips Electronics N.V.  
Groenewoudseweg 1  
NL-5621 BA Eindhoven (NL)

**Representative:** Cohen, Julius Simon  
Philips Intellectual Property & Standards  
P.O. Box 220  
NL-5600 AE Eindhoven (NL)

**Decision under appeal:** Decision of the Examining Division of the  
European Patent Office posted 27 December 2002  
refusing European application No. 96931194.3  
pursuant to Article 97(1) EPC.

**Composition of the Board:**

**Chairman:** T. Kriner  
**Members:** S. Chowdhury  
E. DufRASne

## Summary of Facts and Submissions

- I. This appeal is against the decision of the examining division dated 27 December 2002 to refuse European patent application No. 96 931 194.3.

The ground of refusal was that claims 1 and 5 of the main request and the first auxiliary request and claim 4 of the second auxiliary request then on file related to diagnostic methods performed on the human body, which fell under the exclusion of Article 52(4) EPC, and claims 1 and 5 of the third auxiliary request were unclear.

During the examination procedure the examining division had argued that the subject-matter of claims 6 and 7 lacked novelty having regard to:

D1: "Technical Optimisation of Spiral CT for Depiction of Renal Artery Stenosis: In Vitro Analysis"; Brink J. et al.; Cardiovascular Radiology; 1995; **194**: pages 157-163.

- II. On 13 February 2003 the appellant (applicant) lodged an appeal against the decision and paid the prescribed fee on the same day. On 8 April 2003 a statement of grounds of appeal was filed.

The appellant requests that the decision under appeal be set aside and that a patent be granted on the basis of claims 1 to 4 filed on 24 January 2006, and amended as agreed by telephone on 26 January 2006.

III. IV. Independent claims 1, 3, and 4 read as follows:

"1. A method of measuring a dimension of a detail (20) of an object from a density distribution of the object to be examined

- by using the density distribution of a part (P1) of the object outside said detail, which part (P1) has a dimension which is larger than that of said detail (20) in the object to be examined and

- of which part the density is substantially the same as the density of said detail, wherein

- the maximum value (dmax) of the density distribution of said larger part (P1) is derived,

- a corrected maximum value of the density distribution of said detail is derived from the maximum value (dmax) of said larger part and

- the value of the dimension of the detail (20) in the object is derived from the width of the density distribution of said detail, at a density value amounting to a predetermined fraction of said corrected maximum value.

3. An imaging system including

- a device for reconstructing a density distribution of an object to be examined and

- an arithmetic device arranged to derive a dimension of a detail of the object from the density distribution of the object to be examined

- by using the density distribution of a part (P1) of the object outside said detail, which part (P1) has a dimension which is larger than that of said detail (20) in the object to be examined and

- of which part the density is substantially the same as the density of said detail, wherein the arithmetic device is further arranged to
- derive the maximum value (dmax) of the density distribution of said larger part (P1)
- derive a corrected maximum value of the density distribution of said detail from the maximum value (dmax) of said larger part and
- derive the value of the dimension of the detail (20) in the object from the width of the density distribution of said detail, at a density value amounting to a predetermined fraction of said maximum value (dmax).

4. A computer tomography device, comprising

- an X-ray source (1) for irradiating an object (2) to be examined by means of X-rays,
- an X-ray detector (3) for detecting X-rays having traversed the object to be examined,
- the X-ray source and the X-ray detector being positionable together in a number of orientations relative to the object,
- a reconstruction unit (4) for reconstructing a density distribution of the object to be examined on the basis of X-ray images detected in separate orientations, and
- an arithmetic device (5) arranged to derive a dimension of a detail of the object from the reconstructed density distribution of the object to be examined
- by using the density distribution of a part (P1) of the object outside said detail, which part (P1) has a dimension which is larger than that of said detail (20) in the object to be examined and

- of which part the density is substantially the same as the density of said detail, wherein the arithmetic device is further arranged to
- derive the maximum value (dmax) of the density distribution of said larger part (P1)
- derive a corrected maximum value of the density distribution of said detail from the maximum value (dmax) of said larger part and
- derive the value of the dimension of the detail (20) in the object from the width of the density distribution of said detail, at a density value amounting to a predetermined fraction of said maximum value (dmax)."

Claim 2 is a dependent claim.

IV. The appellant argued as follows:

The independent claims included the feature of the value of the dimension of the detail being derived from both density values of the density distribution of the detail and density values outside the detail, whereas D1 only mentioned computing the diameter of a stenosis model on the basis of the full width at one-tenth maximum (FWTM) or the full width at one-tenth area (FWTA) methods. This did not pertain to the derivation of the dimension of the detail but rather to the relative comparison of sizes of several portions of the density distribution. Hence D1 did not give the skilled person any incentive to change the way the measurement of the stenotic part was made.

The method of the invention was applied to a dataset which was not practised on the living body. The Boards of Appeal had consistently reasoned that steps limited to operation of a technical device falling under the competence of a technician do not fall in the exclusion. The present method relates to the analysis of a dataset and was limited to the operation of an arithmetic unit and was consequently not a diagnostic method within the meaning of Article 52(4) EPC.

### **Reasons for the Decision**

1. The appeal is admissible.
2. *Amendments*

Present claim 1 is based on claims 1 and 2 of the application as originally filed (WO-A-97/13457), amplified by the features that the part (P1) has a dimension which is larger than that of said detail (20) in the object to be examined, and the part has a density which is substantially the same as the density of said detail. These features are supported by page 4, lines 11 to 13 and 23 and 24.

Claim 2 corresponds to original claim 4.

Claims 3 and 4 correspond to original claims 6 and 7, with amendments corresponding to those in claim 1.

All the amendments satisfy the requirement of Article 123(2) EPC, accordingly.

3. *Article 52(4) EPC*

3.1 The headnote of the opinion G 1/04 of the Enlarged Board of Appeal reads, *inter alia*, as follows:

1. In order that the subject-matter of a claim relating to a diagnostic method practised on the human or animal body falls under the prohibition of Article 52(4) EPC, the claim is to include the features relating to:

(i) the diagnosis for curative purposes *stricto sensu* representing the deductive medical or veterinary decision phase as a purely intellectual exercise,

(ii) the preceding steps which are constitutive for making that diagnosis, and

(iii) the specific interactions with the human or animal body which occur when carrying those out among these preceding steps which are of a technical nature.

3. In a diagnostic method under Article 52(4) EPC, the method steps of a technical nature belonging to the preceding steps which are constitutive for making the diagnosis for curative purposes *stricto sensu* must satisfy the criterion "practised on the human or animal body".

3.2 The claimed method does not include any features relating to the diagnosis for curative purposes *stricto sensu* representing the deductive medical or veterinary decision phase as a purely intellectual exercise, nor are the method steps of claim 1 practised on the human or animal body. The presently claimed method pertains



to the analysis of a data set and the information which it yields provides intermediate results which, on their own, do not enable a decision to be made on the treatment necessary.

For these reasons the claimed method is not to be considered a diagnostic method practised on the human or animal body which is excluded from patentability by Article 52(4) EPC.

4. *The application*

The application relates to a method of measuring a dimension of a detail of an object from a density distribution of the object obtained from a shadow image, and to corresponding apparatus.

Such a method known from D1 uses a density distribution profile of the object obtained by computer tomography and measures the FWTM and the FWTA of averaged profiles to determine the dimension of the object. The technical problem with this known method is that owing to blurring of the image, which may be caused by different technical factors (page 2, line 31 to page 3, line 1), the maximum density of the profile of a detail is reduced and the dimension of the detail tends to be overestimated, accordingly.

The solution, as reflected in the method according to present claim 1, is based on the recognition of the fact that relatively larger parts of an object are less affected by the blurring, and uses this fact to compensate for the reduction of the maximum density of the profile of a smaller part of the object, and hence

for the disturbance of the measurement of the dimension owing to blurring of the image.

According to this method the maximum value of the density distribution of the larger part is derived and a corrected maximum value of the density distribution of the smaller part is derived from the maximum value of the larger part. The dimension of the smaller part is then derived from the width of the density distribution of the smaller part, at a density value amounting to a predetermined fraction of the corrected maximum value. In an example the full width of the profile of smaller part of the density distribution of an object is measured, not at the half maximum of the density distribution of the profile of the smaller part itself, but at the half maximum of the density distribution of the profile of the larger part.

5. *Novelty*

D1 describes the construction of computed tomography images of polyester tubes (pipettes) provided with constrictions of different dimensions and filled with an X-ray attenuating liquid. The pipettes simulate vascular constrictions in a patient to be examined, and two pipettes with constrictions of 45% and 85% (Figure 1), corresponding to critical and non-critical artery stenosis, respectively, are examined.

Spiral CT images of the pipettes were made using 12 different scan parameters and scanning techniques, and the results are presented in Figures 3 and 4, respectively for the non-critical and critical artery stenosis.

The diameters of the normal and stenotic portions of the test images were measured from the attenuation profiles, and as measures of tube diameter the FWTM and the FWTA were computed for each profile. The results show that the measured diameters using FWTM and FWTA are consistently too high (Figures 3a, 3b, 4a, 4b).

There is no disclosure in D1 of employing a compensation scheme in which the density profile of a structure that is larger than the object to be measured is used for any reason. For this reason the method of claim 1 is novel over the method disclosed in D1.

6. *Inventive step*

Although D1 recognises that there are various causes for the underestimation or overestimation of tube diameters in spiral CT, it does not discuss the technical problem of the application as set out in point 4, second paragraph above. Nor does D1 disclose the present solution.

Since neither the problem of distortion of the density profile nor the solution of invoking the density profile of a structure that is larger than the detail of the object in order to compensate for the blurring effect is disclosed in D1 the method of claim 1 involves an inventive step.

7. The same arguments apply to the subject-matter of independent Claims 3 and 4, which claim apparatus for implementing the method of claim 1.

**Order**

**For these reasons it is decided that:**

1. The decision under appeal is set aside.
2. The case is remitted to the department of the first instance to grant a patent on the basis of the following documents:
  - Claims 1 to 4 filed by telefax on 24 January 2006, claim 3 being amended as agreed with the representative by telephone on 26 January 2006
  - Description pages 1 and 6 to 10 as published
  - Description pages 2, 3, and 4 filed by letter dated 13 May 2005, page 4 being amended as agreed with the representative by telephone on 26 January 2006
  - Description page 5 filed by telefax dated 24 January 2006
  - Figures 1 to 3 as published.

The Registrar:

The Chairman:

V. Commare

T. K. H. Kriner